

# Assessing delivery and quantifying efficacy of small interfering ribonucleic acid therapeutics in the skin using a dual-axis confocal microscope

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**Abstract.** Transgenic reporter mice and advances in imaging instrumentation are enabling real-time visualization of cellular mechanisms in living subjects and accelerating the development of novel therapies. Innovative confocal microscope designs are improving their utility for microscopic imaging of fluorescent reporters in living animals. We develop dual-axis confocal (DAC) microscopes for such *in vivo* studies and create mouse models where fluorescent proteins are expressed in the skin for the purpose of advancing skin therapeutics and transdermal delivery tools. Three-dimensional image volumes, through the different skin compartments of the epidermis and dermis, can be acquired in several seconds with the DAC microscope in living mice, and are comparable to histologic analyses of reporter protein expression patterns in skin sections. Intravital imaging with the DAC microscope further enables visualization of green fluorescent protein (GFP) reporter gene expression in the skin over time, and quantification of transdermal delivery of small interfering RNA (siRNA) and therapeutic efficacy. Visualization of transdermal delivery of nucleic acids will play an important role in the development of innovative strategies for treating skin pathologies. © 2010 Society of Photo-Optical Instrumentation Engineers. [DOI: 10.1117/1.3432627]

Keywords: confocal fluorescence microscopy; three-dimensional microscopy; *in vivo* imaging; molecular imaging; intravital imaging.

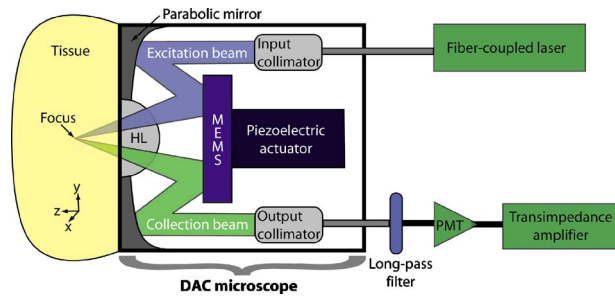
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## 1 Introduction

Advances in molecular probes, transgenic mouse models, and imaging instrumentation as part of the field of molecular imaging are enabling elucidation of *in vivo* cell biology, molecular pathways, and disease mechanisms.<sup>1</sup> Fluorescence imaging techniques are widely used to visualize dynamic biological processes in cells and living animals, but most wide-field microscopes are limited to thin or transparent samples and are largely used on cells and excised tissues. Intravital microscopy, where the microscope objective is placed in proximity to tissues of living animals, is revealing cellular and molecular changes that were previously inaccessible.<sup>2</sup> Recently, we have developed a microelectromechanical systems (MEMS)-based dual-axis confocal (DAC) microscope that performs 3-D cellular imaging in a miniaturized package conducive to *in vivo* imaging for the purpose of improving preclinical studies and enabling clinical point-of-care microscopy.<sup>3</sup> The DAC architecture provides optical sectioning performance with cellular resolution<sup>4</sup> as well as superior rejection of scattered

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**Fig. 1** Schematic of the dual-axis confocal (DAC) microscope system. HL: hemispherical lens; MEMS: microelectromechanical systems scanning mirror; PMT: photomultiplier tube.

light, relative to conventional single-axis confocal microscopes, leading to deeper imaging in tissue.<sup>5,6</sup>

The hand-held DAC microscope is well suited for imaging the skin, where depths down to 150  $\mu\text{m}$  can be acquired non-invasively. This includes the full epidermis and upper dermis of the mouse footpad, which has similar thickness and layer composition to human skin. The genetics of monogenic skin disorders—skin diseases resulting from a single gene mutation—are well characterized and have identified targets for developing molecular therapies.<sup>7</sup> Small interfering RNAs (siRNAs) are promising drug candidates for these disorders due to potency and selectivity for silencing target genes.<sup>8</sup> Despite demonstrated effects of siRNA for controlling gene expression in cultured cells, development of siRNA-based therapies for treating patients, including those with monogenic skin disorders, has largely stalled at the point of effective delivery.<sup>9,10</sup> Our group has previously reported on the development of reporter mouse models enabling the study of siRNA delivery to the skin, where siRNA silencing of the reporter gene was demonstrated.<sup>8,11</sup>

Here, we demonstrate the ability of the hand-held DAC microscope to perform 3-D *in vivo* molecular imaging to study gene expression in mouse skin models and reveal the spatiotemporal gene expression patterns in response to siRNAs targeting the reporter gene. *In vivo* fluorescence signal levels at different time points are quantified as a means of assessing therapeutic response. Intravital imaging in the skin offers the potential for accelerating the development of therapies in dermatology.

## 2 Materials and Methods

### 2.1 Imaging Systems

#### 2.1.1 Dual-axis confocal microscope

The 10-mm-diam DAC microscope is based on a dual-axis architecture<sup>12</sup> and MEMS technology<sup>13</sup> for miniaturization, and has a transverse resolution of 2.5  $\mu\text{m}$  and axial resolution of 5.8  $\mu\text{m}$  at 488-nm wavelength. A schematic of the imaging system is shown in Fig. 1, with the DAC microscope alongside the laser and detection apparatus. Details of the microscope setup and components were previously reported.<sup>3</sup> The 2-D MEMS mirror raster scans the focal volume to generate a 2-D *en face* image (*xy* plane) at 4 fps, while the piezoelectric actuator translates the MEMS scanner in depth (*z* direction) every 2.3  $\mu\text{m}$  to acquire a 3-D dataset, satisfying

the Nyquist sampling rate for cellular optical sectioning. 3-D image stacks were reconstructed into volume renderings using Amira<sup>®</sup> software (Visage Imaging, San Diego, California).

#### 2.1.2 Maestro<sup>™</sup> and IV100

The Maestro<sup>™</sup> optical imaging system (CRi, Woburn, Massachusetts) was used for whole-animal fluorescence imaging. Images were acquired with an excitation filter of 445- to 490-nm wavelength, and a 515-nm long-pass emission filter for imaging green fluorescent protein (GFP). Multispectral image acquisition was performed and later used for spectral unmixing of autofluorescence with the Maestro software.

The Olympus IV100 is a laser scanning microscope for intravital imaging. Images were acquired at 4 fps with a 4 $\times$  objective, and a 488-nm argon laser was used for imaging the levels of GFP expression. Image stacks were taken every 50- $\mu\text{m}$  depth. Image acquisition and viewing were done with the FluoView software (Olympus Corporation, Center Valley, Pennsylvania).

## 2.2 Animal Models and In Vivo Imaging

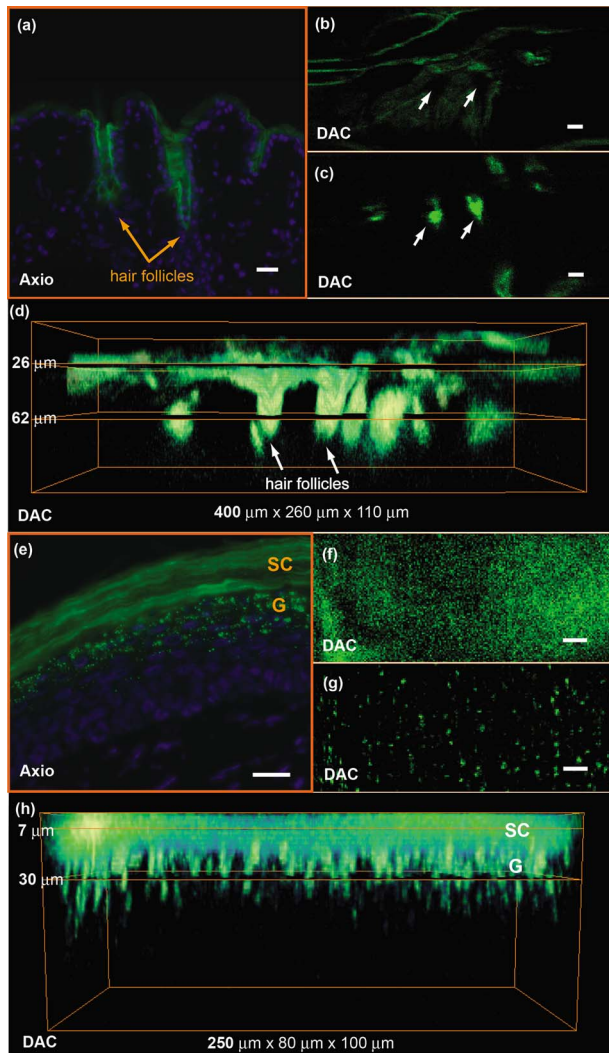
Transgenic mouse models that express GFP in the skin were used. The [mK17 5']-GFP mice (K17-GFP mice) were kindly provided by Coulombe.<sup>14</sup> Skin-specific dual-reporter click beetle luciferase/humanized monster GFP mice (Tg CBL/hMGFP mice) were previously described and maintained in the animal facility at Stanford University.<sup>11</sup> The mice were under 2% isoflurane anesthesia during *in vivo* imaging. For DAC imaging, an optical gel (index of refraction is 1.46) was applied to the region of the skin as an optical coupling agent. All animal work was carried out under strict adherence to institutional guidelines for animal care of both National Institutes of Health and Stanford University.

## 2.3 Quantification

The *in vivo* GFP signal level in a given tissue volume was assessed by AMIDE software.<sup>15</sup> For quantification of DAC images, illumination and detection settings were held constant within and between image datasets. Within the acquired 3-D volume, a region of interest was drawn consistently over different datasets for comparison of mean signal levels.

## 3 Results and Discussion

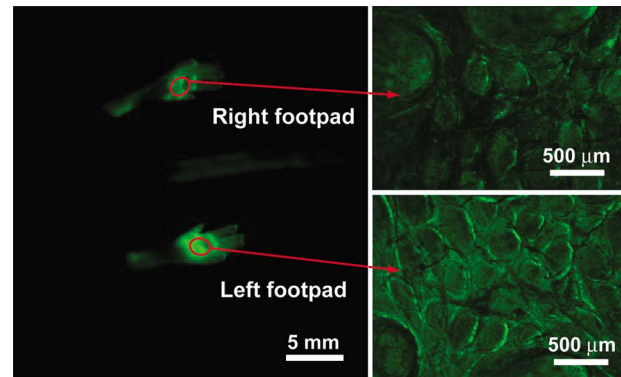
Microscopic images of transgenic mouse skin models are shown in Fig. 2. In these models, GFP is expressed in different compartments of the skin depending on the skin-specific promoter regulating the expression of the reporter protein or the recombinase used to direct skin specificity. These mouse models can be used to target different skin compartments for therapeutic development. Figures 2(a)–2(d) show images from mice where GFP expression is driven by a keratin 17 (K17) promoter.<sup>14</sup> This promoter leads to GFP expression in epithelial structures such as hair follicles and glands. Figure 2(a) is an image of an *ex vivo* vertical skin section from the K17-GFP mouse taken with a conventional microscope (table-top Axio Observer inverted fluorescence microscope). The tissue was removed, frozen, sectioned into 10- $\mu\text{m}$ -thick slices, and stained with DAPI for visualizing nuclei. Strong GFP expression is evident in the hair follicles. In comparison, the



**Fig. 2** Microscopic imaging of transgenic mouse skin models. (a) through (d) are images of skin on the back of the K17-GFP mouse model. (a) *Ex vivo* skin vertical cross section ( $10\ \mu\text{m}$  thick) image taken with a tabletop Axio Observer inverted fluorescence microscope showing GFP (green) signal and DAPI (blue) stain. (b), (c), and (d) *In vivo* imaging with DAC microscope where *en face* images at (b)  $26\ \mu\text{m}$  and (c)  $62\ \mu\text{m}$  depth are shown; these are cross sections of (d) the 3-D tissue volume. (e) through (h) are images of footpad skin of the Tg CBL/hMGFP mouse model. (e) *Ex vivo* skin vertical cross section image taken with a tabletop Axio Observer microscope showing GFP signal and DAPI stain. (f), (g), and (h) *In vivo* imaging with DAC microscope where *en face* images at (f)  $7\ \mu\text{m}$  and (g)  $30\ \mu\text{m}$  depth are cross sections of (h) the 3-D tissue volume. All scale bars are  $20\ \mu\text{m}$ .

DAC microscope was used to image another live K17-GFP mouse, and images of optical sections of the skin are shown in Figs. 2(b) and 2(c). These are single *en face* images acquired at  $26$  and  $62\ \mu\text{m}$  in depth, where the two planes correspond to two cut-away slices from the full 3-D volume rendered in Fig. 2(d).

Figures 2(e)–2(h) are from the Tg CBL/hMGFP mouse model, where hMGFP is localized in the top layers of the epidermis—the *stratum corneum* (SC) and granular layer (G).<sup>11</sup> The *ex vivo* skin section is shown in Fig. 2(e), where the expression pattern in the *stratum corneum* appears uni-

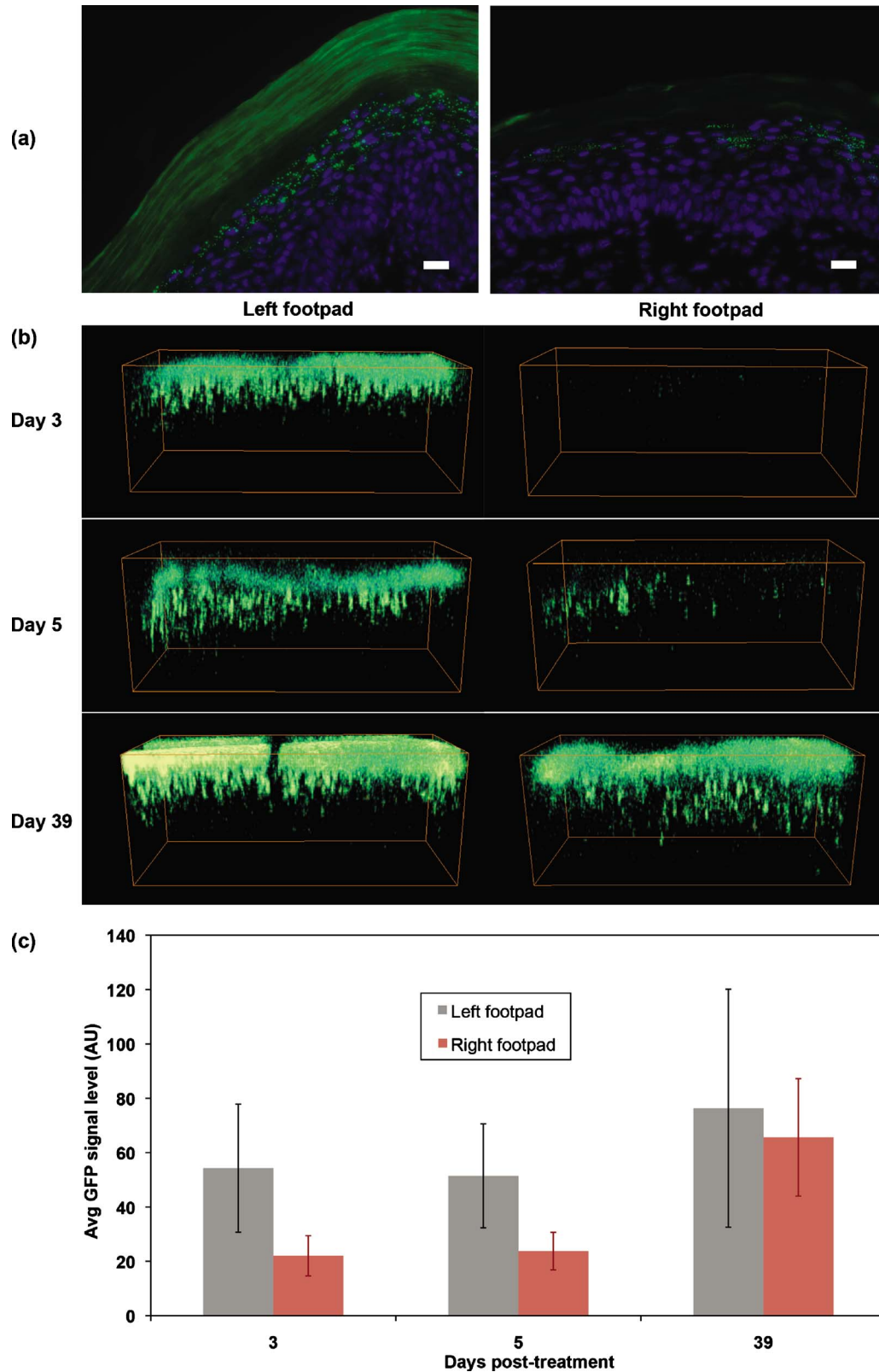


**Fig. 3** SiRNA silencing visualized by macro- and mesoscopic intravital imaging 4 days post-treatment of a Tg CBL/hMGFP mouse. Irrelevant control siRNA (left footpad) and specific siRNA (right footpad) were injected intradermally at daily intervals for 3 days. Left panel: macroscopic image taken with CRI Maestro™. Right panel: mesoscopic images taken with Olympus IV100.

form, and in the granular layer appears as aggregates. Figures 2(f) and 2(g) show *in vivo* DAC images from another live mouse at  $7$  and  $30\ \mu\text{m}$  depth corresponding to the SC and G layers, respectively. Each plane can be identified in the 3-D tissue volume shown in Fig. 2(h). These figures demonstrate that the DAC microscope not only performs molecular imaging with cellular resolution *in vivo*, but can also acquire full-perspective 3-D volumes that are difficult to attain with skin sections. It should be noted that the high dynamic range and sensitivity of the microscope allows for imaging GFP expression at depths that are relevant to the study of skin pathologies and response to therapy.

The Tg CBL/hMGFP mouse [Figs. 2(e)–2(h)] was previously developed as a model in which to test delivery tools for treating monogenic skin disorders.<sup>11</sup> Delivery technologies aimed at directing siRNA into skin cells at relevant layers of the skin can be tested in this mouse model, since the use of siRNA targeting GFP would enable gene silencing effects to be readily visualized, i.e., decrease in fluorescence signal at the site of delivery. The effects of this localized gene silencing can be initially observed in macro- and mesoscopic intravital images (Fig. 3, left and right panels, respectively). The Tg CBL/hMGFP mouse was treated daily for three days with intradermal injections of  $100\ \mu\text{g}$  of specific siRNA (CBL3,<sup>11</sup> right footpad) targeting GFP and compared to an irrelevant siRNA (K6a 513a.12,<sup>11</sup> left footpad). At the fourth day post-treatment, a maximum decrease in GFP signal was observed macroscopically with Maestro™ (Fig. 3, left panel). Then, the middle regions of the footpads, at the site of siRNA injections, were imaged with the IV100 microscope (Fig. 3, right panel) for better visualization of GFP inhibition in the right footpad. Although these images show the gene silencing effect of the specific siRNA treatment compared to the irrelevant control siRNA treatment *in vivo*, it is difficult to assess protein expression at the cellular level, and to quantify the GFP signal over time.

Microscopic images of *ex vivo* skin sections from a Tg CBL/hMGFP mouse, after two weeks of daily intradermal injections of  $60\text{-}\mu\text{g}$  siRNA, reveal gene knockdown [Fig. 4(a)]. While a normal pattern of GFP expression can be seen



**Fig. 4** SiRNA silencing visualized at the microscopic level in the Tg CBL/hMGFP mouse model. Irrelevant control siRNA and specific siRNA were injected intradermally into the left and right footpad, respectively. (a) *Ex vivo* skin sections after two weeks of treatment. Scale bars are 20  $\mu\text{m}$ . (b) *In vivo* imaging of footpads after 18 days of treatment using the DAC microscope. Sequential time points correspond to days post-treatment. The 3-D volume dimensions are  $250 \times 80 \times 100 \mu\text{m}^3$ . (c) Quantification of GFP signal levels from image stacks taken with the DAC microscope. Each footpad at each timepoint is imaged over multiple sites. Each column corresponds to the average of the datasets, and bars indicate the standard deviation. For days 3 and 5, the difference between left and right footpad are statistically significant, while for day 39, the difference is not statistically significant.

for the left footpad (irrelevant control siRNA), the right footpad (specific siRNA) demonstrates significant inhibition of GFP expression. However, using traditional fluorescence microscopy of skin sections, we can only observe one time-point per mouse. To visualize change over time with this method, multiple mice would need to go through the same procedure and be sacrificed at different time points to study the dynamic response to therapy and restoration of expression. Mouse-to-mouse variability is generally hard to account for in these scenarios.

The DAC microscope allows for sequential cellular level imaging and quantification *in vivo*. The previous siRNA experiment was replicated with a Tg CBL/hMGFP mouse that was treated over 18 days and was followed post-treatment with the DAC microscope. The anesthetized mouse was imaged in multiple locations on each footpad. Since the left footpad (irrelevant control siRNA) appeared to have uniform fluorescence under the DAC microscope, image stacks were taken around the general area of intradermal injections in the mid-region of the footpad, corresponding to the area shown in the right panel of Fig. 3. For the right footpad (specific siRNA), the DAC microscope was used to scan an area of decreased GFP signal and acquire 3-D datasets over multiple sites. Representative 3-D image volumes taken in the mid-region at different time points post-treatment are shown in Fig. 4(b). The GFP expression levels are significantly lower in the specific siRNA-treated right footpad compared to the normal expression of the left footpad at day 3 post-treatment. However, since siRNA silencing is inherently a transient response, the GFP signal recovers some time after the treatment ends. This can be clearly seen at day 39 post-treatment. The laser power and PMT, transimpedance amplifier gain levels (Fig. 1), are controlled to be constant within and between datasets. Therefore, all volume renderings in Fig. 4(b) show levels of GFP *in vivo* that can be compared over time. A subset of the 3-D volume was taken into account for quantification, where the skin layer thickness and attributes are consistent. Fig. 4(c) shows the average GFP signal levels of the left and right footpad for the days represented in Fig. 4(b). At days 3 ( $p=0.0028$ ) and 5 ( $p=0.0020$ ) post-treatment, we observed statistically significant GFP inhibition in the right footpad, indicative of gene silencing. On day 39 post-treatment ( $p=0.3623$ ), the signal level for the right footpad recovered to similar levels of the left footpad. We note that the ratios of the average GFP signal of the right to left footpad are 40.6, 46.2, and 85.9% for days 3, 5, and 39 post-treatment, as expected as the therapeutic effect wanes. This form of quantification of sequential *in vivo* gene expression gives us an opportunity to directly monitor the effects of therapy.

We demonstrate here the ability of the miniature DAC microscope to perform quantitative *in vivo* 3-D molecular imaging in skin. The high dynamic range of the microscope enables imaging of gene expression deep in tissue. With the capability to noninvasively image throughout the epidermis, effects of siRNA therapy on skin cells have been directly monitored. This can serve as a platform for tracking the progress and efficacy of drug candidates and delivery mechanisms over time.

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## References

1. N. Blow, "In vivo molecular imaging: the inside job," *Nat. Methods* **6**, 465–469 (2009).
2. R. K. Jain, L. L. Munn, and D. Fukumura, "Dissecting tumour pathophysiology using intravital microscopy," *Nat. Rev. Cancer* **2**, 266–276 (2002).
3. H. Ra, W. Piyawattanametha, M. J. Mandella, P. L. Hsiung, J. Hardy, T. D. Wang, C. H. Contag, G. S. Kino, and O. Solgaard, "Three-dimensional *in vivo* imaging by a handheld dual-axes confocal microscope," *Opt. Express* **16**, 7224–7232 (2008).
4. E. González-González, H. Ra, R. Spitzer, R. P. Hickerson, C. H. Contag, and R. L. Kaspar, "Increased interstitial pressure improves nucleic acid delivery to skin enabling a comparative analysis of constitutive promoters," *Gene Ther.* (in press).
5. L. K. Wong, M. J. Mandella, G. S. Kino, and T. D. Wang, "Improved rejection of multiply scattered photons in confocal microscopy using dual-axes architecture," *Opt. Lett.* **32**, 1674–1676 (2007).
6. J. Liu, M. J. Mandella, J. Crawford, C. H. Contag, T. D. Wang, and G. S. Kino, "Efficient rejection of scattered light enables deep optical sectioning in turbid media with low-numerical-aperture optics in a dual-axis confocal architecture," *J. Biomed. Opt.* **13**, 034020 (2008).
7. S. A. Leachman, R. P. Hickerson, P. R. Hull, F. J. D. Smith, L. M. Milstone, E. B. Lane, S. J. Bale, D. R. Roop, W. H. I. McLean, and R. L. Kaspar, "Therapeutic siRNAs for dominant genetic skin disorders including pachyonychia congenita," *J. Dermatol. Sci.* **51**, 151–157 (2008).
8. R. P. Hickerson, F. J. D. Smith, R. E. Reeves, C. H. Contag, D. Leake, S. A. Leachman, L. M. Milstone, W. H. I. McLean, and R. L. Kaspar, "Single-nucleotide-specific siRNA targeting in a dominant-negative skin model," *J. Invest. Dermatol.* **128**, 594–605 (2008).
9. U. R. Hengge, "Gene therapy progress and prospects: the skin—easily accessible, but still far away," *Gene Ther.* **13**, 1555–1563 (2006).
10. S. A. Leachman, R. P. Hickerson, M. E. Schwartz, E. E. Bullough, S. L. Hutcherson, K. M. Boucher, C. D. Hansen, M. J. Eliason, G. S. Srivatsa, D. J. Kornbrust, F. J. Smith, W. I. McLean, L. M. Milstone, and R. L. Kaspar, "First-in-human mutation-targeted siRNA phase Ib trial of an inherited skin disorder," *Mol. Ther.* **18**, 442–446 (2010).
11. E. González-González, H. Ra, R. P. Hickerson, Q. Wang, W. Piyawattanametha, M. J. Mandella, G. S. Kino, D. Leake, A. Avilion, O. Solgaard, T. Doyle, C. H. Contag, and R. L. Kaspar, "siRNA silencing of keratinocyte-specific GFP expression in a transgenic mouse skin model," *Gene Ther.* **16**, 963–972 (2009).
12. T. D. Wang, M. J. Mandella, C. H. Contag, and G. S. Kino, "Dual-axis confocal microscope for high-resolution *in vivo* imaging," *Opt. Lett.* **28**, 414–416 (2003).
13. H. Ra, W. Piyawattanametha, Y. Taguchi, D. Lee, M. J. Mandella, and O. Solgaard, "Two-dimensional MEMS scanner for dual-axes confocal microscopy," *J. Microelectromech. Syst.* **16**, 969–976 (2007).
14. N. Bianchi, D. Depianto, K. McGowan, C. Gu, and P. A. Coulombe, "Exploiting the keratin 17 gene promoter to visualize live cells in epithelial appendages of mice," *Mol. Cell. Biol.* **25**, 7249–7259 (2005).
15. A. M. Loening and S. S. Gambhir, "AMIDE: a free software tool for multimodality medical image analysis," *Mol. Imaging* **2**, 131–137 (2003).